In the first of a series of articles, Professor Paul Tipton gives us an introduction to high performance polymers in dentistry. Here he discusses polyether ether ketone (PEEK), a new material for framework fabrication in prosthodontics.

The high-performance polymers (HPPs) are the uppermost class of plastics, possessing better temperature and chemical stability and mechanical properties than the commodity plastics, but typically being manufactured in lower volumes and costing more.

The family of HPPs that have entered dentistry are called the Polyaryl etherketones (‘PAEKs’), of which there are several members with varying chemical structures. Many of us in the dental industry are inadvertently familiar with the family member called PEEK (Polyetheretherketone), through its use in healing caps, temporary abutments and scan bodies.

However, the reason for the recent enthusiasm surrounding PAEKs has been their potential for use as a metal alternative in broader indications such as removable dentures (Figures 1 and 2) and implant borne prosthetics (Figure 3). It is here that the shock absorbing characteristics of the material could be extremely interesting for immediate loading or long term frameworks (Figure 4).

In this first article of a series of six, the background to these materials will be described. This will be followed by a series of case studies describing their use in removable and implant-borne prosthetics.

The PAEK family
PEEK is the most well-known and most widely used PAEK family member. PEEK was invented in the UK in 1978 (ICI – now as Victrex plc) and was selected by aerospace, semiconductor, automotive and medical industries as a standard material of use in all these sectors. It is typically used as a metal replacement, due to its strength to weight ratio and corrosion resistance. Other family members also exist which are variations of the chemistry (eg PEK and PEKK), and these materials can also be filled with pigments or reinforcing agents. In their unaltered, unfilled state the materials are beige in colour.

PAEKs in Medical
Several of the properties of PEEK that were being exploited in industry (eg strength-to-weight ratio, chemical and wear resistance, radiolucrency, and reduced stiffness versus metals) were naturally intriguing for medical use. The first published PEEK medical research came in the 1980s (Williams et al., 1987) followed by the first implantable grade from Invibio Biomaterial Solutions in the 1990s (Victrex plc./Invibio Ltd, UK). Medical grades have a much tighter specification, and increased quality control than industrial grade materials, which is important in the wake of the silicone breast implant scandal (see http://www.nhs.uk/conditions/breast-implants/pages/pip-introduction.aspx). PEEK remained the only medical PAEK for many years.

Spine surgeons particularly adopted Invibio’s PEEK, liking the reduced Young’s Modulus (stiffness) of the material and the scatter-free CT and MRI imaging. PEEK has since become the standard alternative to titanium for load bearing spinal cage devices for the spine. Today, manufacturer Invibio claims PEEK has been used in around five million implantable devices, spanning some 500 separate US FDA 510k regulatory clearances. In more recent years, additional versions of PEEK and PEKK have appeared on the medical marketplace, but have been limited in use.

PAEKs in dentistry
Short term devices such as temporary healing caps and abutments have been sold direct to dentists through the dental companies for many years. In these situations, either unfilled PEEK or PEKK with a 10% titanium dioxide pigment filler are typical and have been used in these
In the case of customised prostheses, the upstream material or shape becomes the ‘device’ and is regulated and cleared for use for a defined set of indications. Here, the PAEKs have appeared as materials for use in injection press systems or as discs for computer aided design/manufacture (CAD/CAM).

**Types of PAEKs for prosthetics**

There are now many brands of PAEK dental devices becoming available for use in prosthetic frameworks. The most common formulations of the PAEKs are:

- Unfilled, pure 100% PEEK (eg JUVORA, Invibio/JUVORA Ltd). This is a beige material.
- 80% PEEK with 20% nanoceramic filler (eg. BioHPP, Bredent GmbH). This is a white material.
- 80% PEEK with 20% titanium dioxide filler (eg Dentokeep disc, NT Trading). This is a white material.
- 80% PEKK with 20% filler including titanium dioxide (eg Pekkton Ivory, Cendres and Mettaux). This is an off-white material.

Typically the particle size of these fillers (circa. 300-500 nanometers for the nanoceramic) is not likely to give significant reinforcing properties to the material, since they are not fibres. Instead the fillers act more as a pigment and alter surface topography. These levels of 20% filler will make the material stiffness slightly higher, but consequently also slightly increase brittleness. It should also be noted that the inclusion of titanium dioxide mean that the different materials and forms may have varying clearances.

**Methods of framework manufacture**

There are two methods for laboratories to manufacture substructure frameworks from PAEKs. These are: (i) injection moulding or (ii) CAD/CAM.

(i) Industrial injection moulding machines process the polymer under very high speed and pressure (eg. 1000’s bar), which are typically two orders of magnitude higher than the typical bench top pressing machines available to the dental laboratory (eg. 10’s bar). This means that small scale injection moulding of PAEK is no mean feat, due to tight processing windows and design limitations. Also these re-melting of PAEKs can also increase the risk of unpredictable mechanical and physical...
properties (e.g., brittleness, flexibility, colour, warping) if the framework has not cooled and recrystallised correctly.

Finally, re-melting of PAEK materials can also cause degradation of the polymer (e.g., generation of phenol) unless very closely controlled using the correct equipment. This polymer degradation can be accentuated by the inclusion of fillers in the materials (such as reinforcing agents or pigments). Therefore, melt processing of these materials should only be done by a competent laboratory and using the equipment recommended by the supplier.

(ii) The alternative manufacture route uses CAD/CAM technology. This manufacturing route avoids all of the risks mentioned previously for re-melting the polymer. The material properties remain consistent and the framework manufacture can also benefit from the increase precision and reproducibility of a digital workflow. Although it does require a more significant capital investment by the laboratory, many laboratories are seeing that it is necessary to align with other industries and adopt digitisation to increase efficiencies.

PAEK materials further extend these CAD/CAM efficiencies when compared to milling metal substructures, since there is typically less tool wear and faster milling times and the capital equipment necessary to mill them does not need to be as expensive as machines for milling metal frameworks.

It is the author’s view that the optimum use of these materials only comes from the CAD/CAM milling process as opposed to the injection moulding process.

**Polymer properties**

When handling a prosthetic framework made from a PAEK, a striking thing is the difference in weight. When identical full arch implant prosthetic substructure frameworks were made from four different materials, the results from weighing were: PAEK 4.9g, titanium 17g, zirconia 23g and cobalt chrome 33g.

However, it is the possibility to introduce shock absorption to a prosthesis that is perhaps the most exciting. This could have positive implications for patient comfort and for damage limitation. In my view, the most relevant mechanical property related to the aspect of shock absorption is not ultimately compressive strength (as is sometimes promoted), but actually flexural strength and elastic modulus.

Obtaining an increasingly stronger material becomes academic since clearly it would be simplistic to prefer the highest value.

Metals have very high compressive strengths relative to PAEKs but are not shock absorbing. Naturally, a design must also consider the influence of thickness and shape as well, but values for flexural strength and elastic modulus are more indicative of the stiffness of a material and how much it will deflect the load. Stiffer materials, like metals, have a high elastic modulus (see Table 1) meaning that metals require high loads to elastically deform them. Therefore, one can look at natural materials like bone for clues as to an ideal for stiffness. Common denture materials like PMMA have an elastic modulus range of 1.8–3.1 GPa, but limited strength. The
PAEKs have an elastic modulus closer to bone (4-5GPa) allowing the framework to be stiffer, yet still shock absorbing. However, PAEKs also additionally possess sufficient strength to be considered as a metal alternative.

Conclusions
The high-performance polymers called PEEK and PEKK have exciting potential in dentistry as a metal alternative for removable and implant prosthetic frameworks. Their stiffness properties confer promise as a substructure that could add an element of shock absorption. This may have benefits for patient comfort, addressing parafunction and damage limitation. In the following series of case studies, I shall describe the use of a PEEK high performance polymer as a framework for removable and implant prosthetics.

References